Amendments to the Claims:

This listing of claims will replace all prior versions, and listings, of claims in the application:

Listing of the Claims:

- 1. (Currently Amended) An *in vitro* method for the production of a homologous heart valve, comprising the steps of:
 - a) providing a biodegradable support <u>comprising a broad edge</u>,
 - b) colonizing the support with homologous fibroblast or myofibroblasts cells or a combination thereof to form a connective tissue matrix,
 - optionally colonizing the connective tissue matrix with endothelial cells,
 and
 - d) fixing the connective tissue matrix to a non-degradable or poorly degradable frame construction,

wherein, before or after the fixing of the frame construction, the connective tissue matrix optionally colonized with endothelial cells is introduced into a pulsatile flow chamber in which it can be exposed to increasing flow rates, and the flow rate is increased continuously or discontinuously.

- 2. (Currently Amended) An *in vitro* method for the production of a homologous heart valve, comprising the following steps:
 - a) providing a biodegradable support which is firmly connected to a non-degradable or poorly degradable frame construction, wherein the biodegradable support comprises a broad edge,
 - b) colonizing the support with homologous fibroblast or myofibroblasts cells or a combination thereof to form a connective tissue matrix,
 - c) optionally colonizing the connective tissue matrix with endothelial cells,
 - d) introducing the frame construction with the connective tissue matrix connected thereto into a pulsatile flow chamber in which it can be exposed to increasing flow rates, and
 - e) continuously or discontinuously increasing of the flow rate.

- 3. (Previously Presented) The method according to claims 1 or 2, wherein the biodegradable support comprises a biodegradable polymer matrix or an acellular biological matrix.
- 4. (Previously Presented) The method of claim 3, wherein the support comprises a polyglycolic acid (PGA), polylactic acid (PLA), polyhydroxyalkanoate (PHA), poly-4-hydroxybutyrate (P4HB) or a mixture of two or more of these polymers.
- 5. (Previously Presented) The method according to claims 1 or 2, wherein the support has a polymer density of 40 to 120 mg/cm³.
- 6. (Previously Presented) The method according to claims 1 or 2, wherein the support comprises a porous polymer having a pore size of 80 to 240 μm.
- 7. (Previously Presented) The method according to claims 1 or 2, wherein the fibers of the support have a diameter of 6 to 20 μm .
- 8. (Previously Presented) The method of claim3, wherein the support comprises an acellular connective tissue framework of an animal or human heart valve.
- 9. (Previously Presented) The method according to claims 1 or 2, wherein the step of colonization with fibroblast or myofibroblasts cells or a combination thereof repeated 3 to 14 times.
- 10. (Previously Presented) The method according to claims 1 or 2, wherein approximately 10^5 to 6 x 10^8 fibroblast or myofibroblasts cells or a combination thereof are employed per square centimeter of support.
- 11. (Previously Presented) The method according to claims 1 or 2, wherein the step of colonization with endothelial cells is repeated 3 to 14 times.

- 12. (Previously Presented) The method according to claims 1 or 2, wherein approximately- 10^5 to 5 x 10^8 endothelial cells are employed per square centimeter of support.
- 13. (Previously Presented) The method according to claims 1 or 2, wherein the cells are human cells.
- 14. (Previously Presented) The method according to claims 1 or 2, wherein the cells are autologous cells.
- 15. (Previously Presented) The method according to claims 1 or 2, wherein the frame construction comprises a biocompatible material.
- 16. (Cancelled)
- 17. (Previously Presented) The method according to claims 1 or 2, wherein the support is fixed to the frame construction by means of conventional suturing, fibrin adhesive, or a combination thereof.
- 18. (Previously Presented) The method according to claims 1 or 2, wherein flow rates of 5 ml/min to 8,000 ml/min are established in the pulsatile flow chamber.
- 19. (Previously Presented) The method according to claims 1 or 2, wherein the flow rate is increased over a period of 1 week to 12 weeks.
- 20. (Previously Presented) The method according to claims 1 or 2, wherein the initial flow rate is 50 to 100 ml/min.
- 21. (Previously Presented) The method according to claims 1 or 2, wherein the initial pulse frequency is 5 to 10 pulses/min.

- 22. (Previously Presented) The method according to claims 1 or 2, wherein the flow rate is increased to 5,000 ml/min.
- 23. (Previously Presented) The method according to claims 1 or 2, wherein the pulse frequency is increased to 180 pulses/min.
- 24. (Previously Presented) The method according to claims 1 or 2, wherein systemic pressures of 10 to 240 mm Hg are established in the pulsatile flow chamber.
- 25. (Previously Presented) An autologous heart valve that has been produced by the method according to claims 1 or 2.
- 26. (Currently Amended) An autologous heart valve having a connective tissue inner structure surrounded by an endothelial cell layer, wherein the connective tissue inner structure is fixed to a non-degradaable or slowly degradable frame construction, wherein the frame construction comprises a broad edge.
- 27. (Previously Presented) The autologous heart valve according to claim 26, wherein a collagen density of 20 to 60 % exists in the connective tissue inner structure.
- 28. (Previously Presented) The autologous heart valve according to claim 27, wherein the heart valve withstands the flow conditions in the human heart.